



Signal Processing for Medical Applications – Frequency Domain Analyses

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Coherence

- The coherence analysis is an extensively used method to study the correlations in frequency domain, between two simultaneously measured signals.
- Let $x(t)$ and $y(t)$ be two simultaneously recorded data sets of length N
- We estimate the short-time power spectra of s_{xx} , s_{yy} , and cross-spectrum, s_{xy} which is the Fourier transform of the cross-correlation function of the signals $x(t)$ and $y(t)$ in each segment.
- Finally, we average the power spectra and the cross-spectrum across all the segments and calculate the coherence as follows:

$$C(\omega) = \frac{|s_{xy}(\omega)|^2}{s_{xx}(\omega) s_{yy}(\omega)} \quad (4.1)$$

Lecture 4 – Different windows used for estimation

Significance of Coherence

- The coherence spectrum represents the strength of correlation between two signals, $x(t)$ and $y(t)$.
- The confidence limit for coherence at the 100 % α is given by

$$C_L = 1 - (1 - \alpha)^{1/(M-1)} \quad (4.2)$$

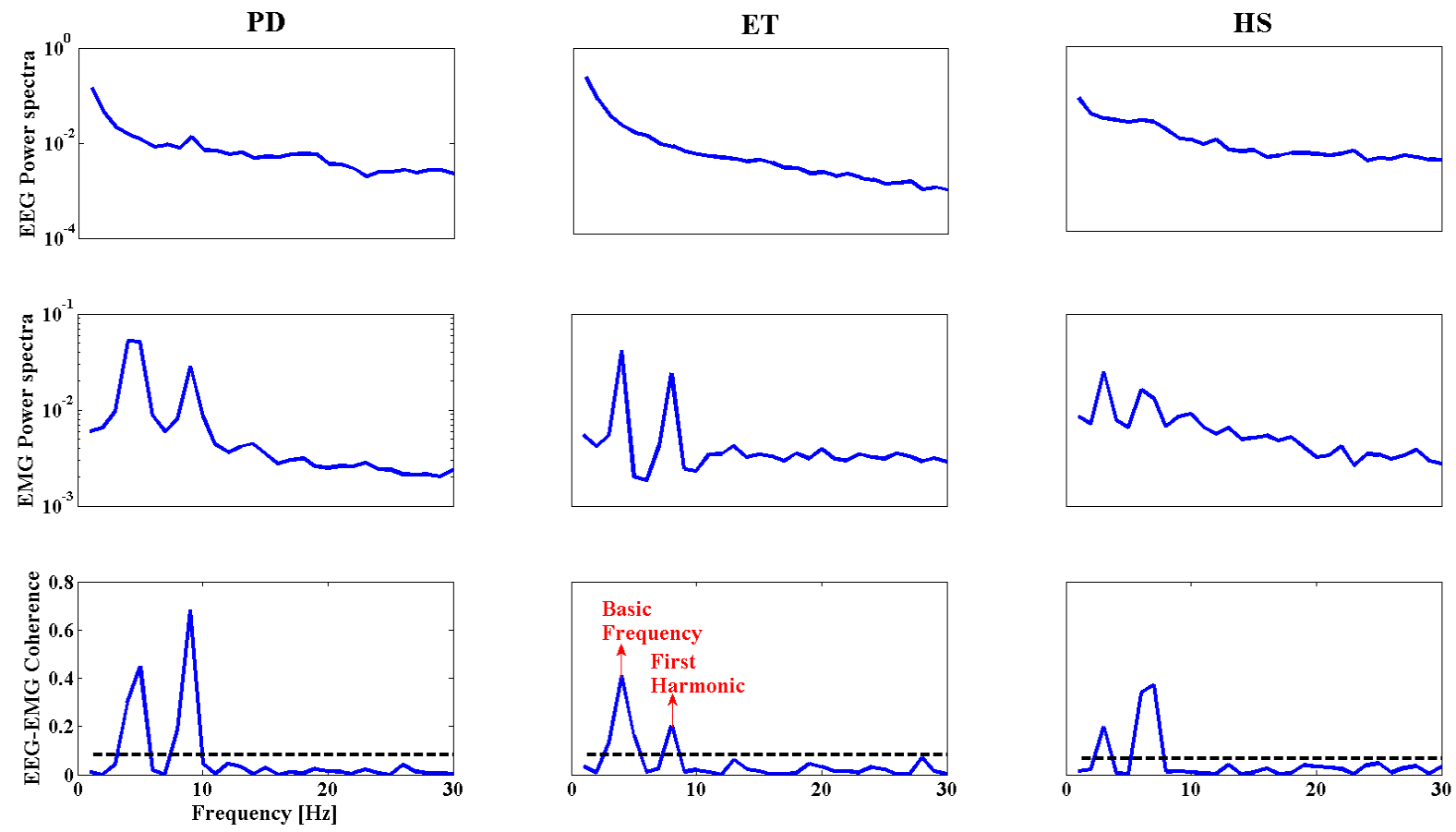
$\alpha = 0.99$; and M is the number of disjoint segments;

hence the confidence limit is $1 - 0.01^{1/(M-1)}$.

- If the signal length $N = 10000$; $D = 1000$; $C_L = ?$;
- Frequency resolution \rightarrow If f_s (i.e. the number of data points sampled per second) is the sampling frequency, then the frequency resolution is f_s/D .
- Thus, one should optimally choose the value of D depending on the purpose of analysis, to compromise between sensitivity and reliability.

Lecture 4 – Different windows used for estimation

Significance of Coherence

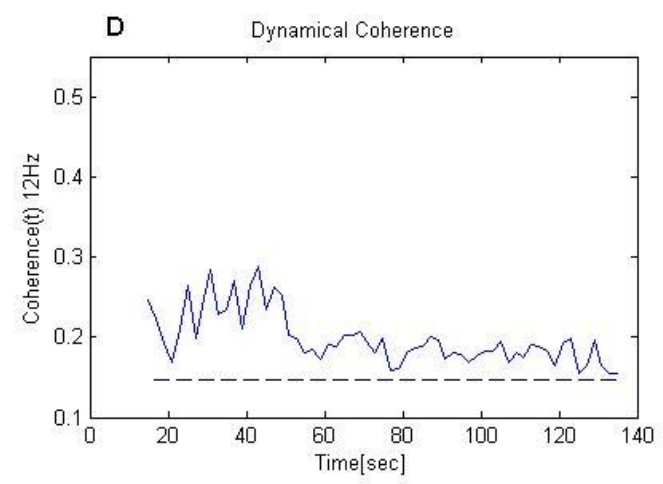
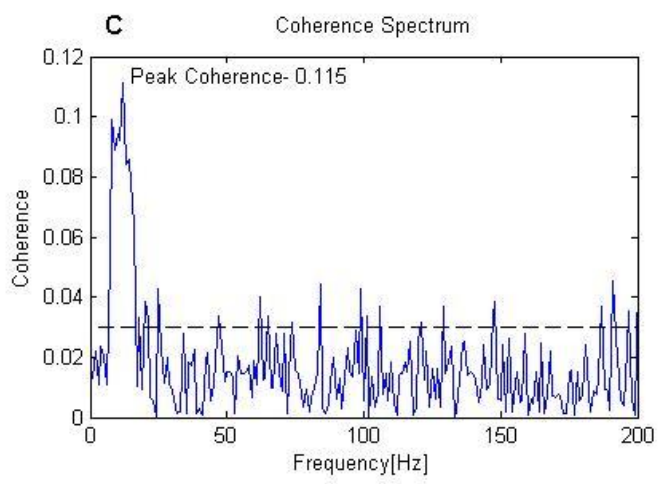
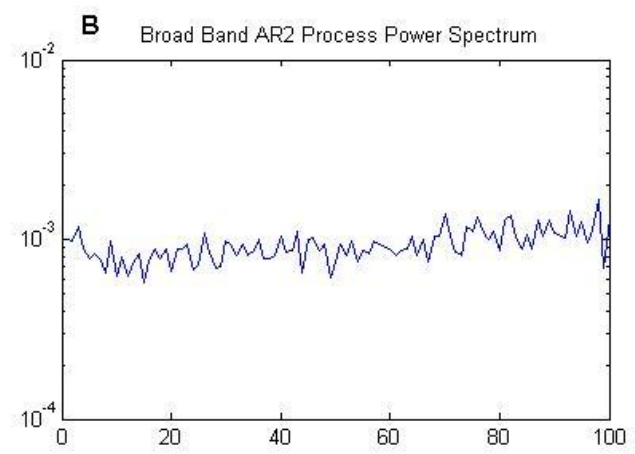
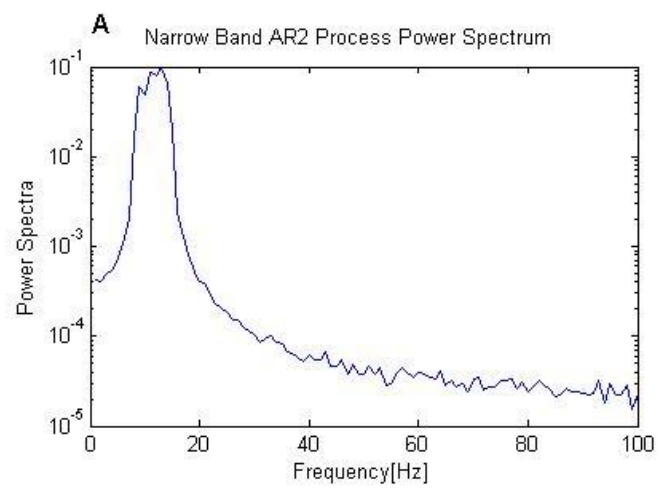


Dynamical Coherence

- The dynamical coherence analysis is done by estimating the coherence spectra for a moving 30-second windows with an overlap of 28-seconds, resulting in an apparent time resolution of 2s.
- A model is created by coupling two AR2 processes $y[n] = a_1 y[n-1] + a_2 y[n-2] + \eta[n]$. One AR2 (V1) had narrow band characteristics ($a_1 = 1.9691, a_2 = -0.9753$) and the other (V2) had broadband spectral characteristics ($a_1 = 0.37486, a_2 = -0.36788$).
- These two processes were simulated for a duration of 150 seconds at a sampling rate of 1,000 Hz. The narrow band AR2 was then band-pass filtered around its spectral peak between 8 and 15 Hz and then combined by point-by-point summation with the broadband AR2 (V2) as follows: $V = V2 + 0.2 V1$.
- Independent white noises were added to V and V1 whose amounts were tuned so that overall coherence between V and V1 was around 0.1.

Lecture 4 – Different windows used for estimation

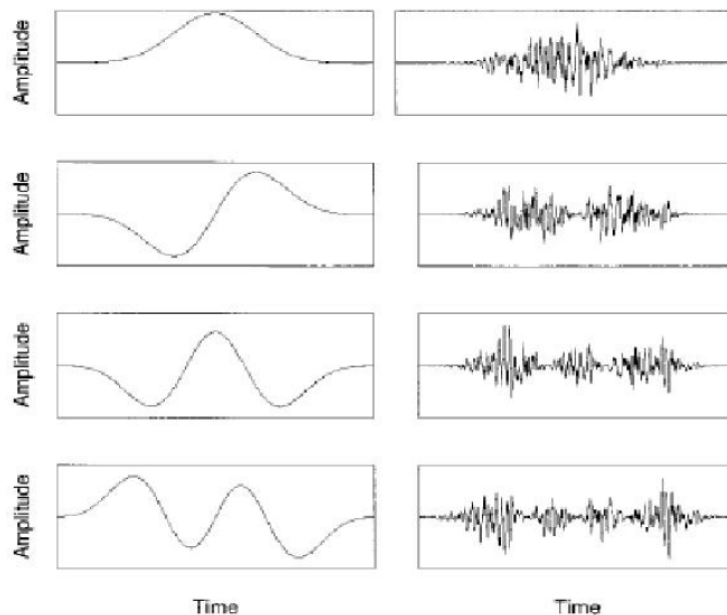
Dynamical Coherence



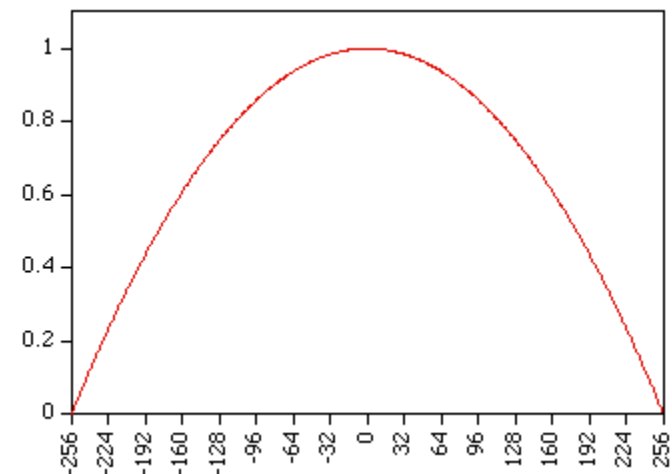
Welch periodogram and Multitaper Method

- Estimation of coherence with these two methods which work on the same principle
- ➔ Multitaper Method with single hanning taper ➔ Hanning window in Welch periodogram Method

Tapers



Hanning Window



Increasing Time Resolution

- If we consider a finite length sample of a discrete time process $x(t)$, $t = 1, 2, \dots, N$. Let us assume a spectral representation for the process,

$$x(t) = \int_{-1/2}^{1/2} X(f) \exp(2\pi i f t) df \quad (4.3)$$

- The Fourier transform $\tilde{x}(f)$ of the data sequence is therefore given by

$$\tilde{x}(f) = \sum_1^N x(t) \exp(-2\pi i f t) = \int_{-1/2}^{1/2} K(f - f', N) X(f') df' \quad (4.4)$$

- The Welch periodogram method is capable of also analysing the signals using larger time windows in the time domain which in turn gives a good estimation of the signal components.
- However, when shorter time windows need to be used, some disadvantages of this method become evident when applied to non-linear signals.
- In this case for a stationary process, the spectrum is given by

$$S(f) df = E\left[|X(f)|^2\right] \quad (4.5)$$

Lecture 4 – Different windows used for estimation

Increasing Time Resolution

- A simple estimation of the spectrum (apart from the normalization constant) is obtained by squaring the Fourier transform of the data sequence, i.e; $|\tilde{x}(f)|^2$.
- This suffers from two difficulties:
 - Firstly, $\tilde{x}(f)$ is not equal to $X(f)$, except when the data length is infinite, in which case the kernel in equation (4.5) becomes a delta function. Rather it is related to $X(f)$ by a convolution as given in equation (4.4).
 - This problem is usually referred to as „bias“ corresponding to a mixing of information from different frequencies of the underlying process due to a finite window length.
 - Secondly, if the data are stochastic, then the squared Fourier transform of a time series is an inconsistent estimator of the spectrum, because it does not converge to the „true“ spectrum when the data series tends to infinite length.
- In order to overcome all these disadvantages, the signals can be analysed with the multitaper and the extended continuous wavelet-transform method.

Multitaper Method

- If $x(t)$ is the signal then the spectrum in this method is calculated by multiplying the data with several orthogonal tapers (windows)

$$S_{MT}(\omega) = \frac{1}{K} \sum_{k=1}^K \left| \tilde{X}_k(\omega) \right|^2 \quad (4.6)$$

where $\tilde{X}_k(\omega)$ is the Fourier transform

$\left[X(\omega) = \int_{-\infty}^{\infty} x(t) \exp(-2\pi i \omega t) dt \right]$ of the data $x(t)$

$$\tilde{X}_k(\omega) = \sum_{t=1}^N w_t(k) x_t \exp(-2\pi i \omega t) \quad (4.7)$$

where $w_t(k) (k = 1, 2, \dots, K)$ are the K orthogonal tapers.

- A particular choice of these taper functions, with optimal spectral concentration properties, is given by the discrete prolate spheroidal sequences (DPSS).

Multitaper Method

- Let $w_i(k, W, N)$ be the k^{th} DPSS of length N and frequency bandwidth parameter W
- Consider a sequence w_i of length N whose Fourier transform is given by $U(\omega) = \sum_1^N w_i \exp(-2\pi i \omega t)$, we find the sequences w_i so that the spectral amplitude $U(\omega)$ is maximally concentrated in the interval $[-W, W]$, i.e.

$$\int_{-W}^W |U(f)|^2 df \quad (4.8)$$

is maximised.

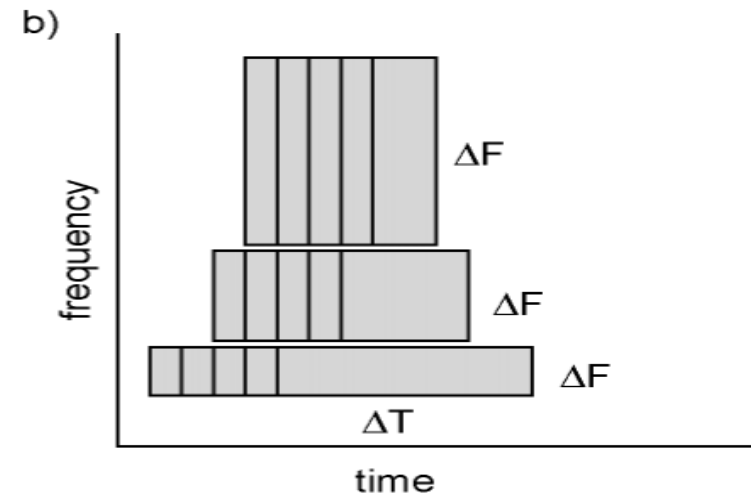
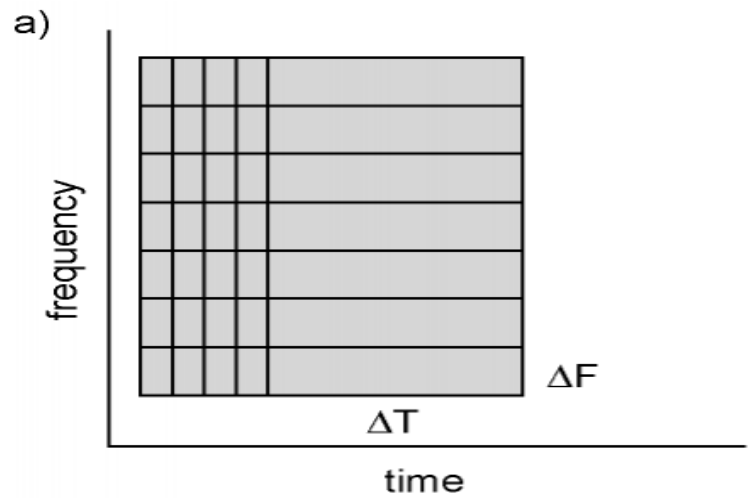
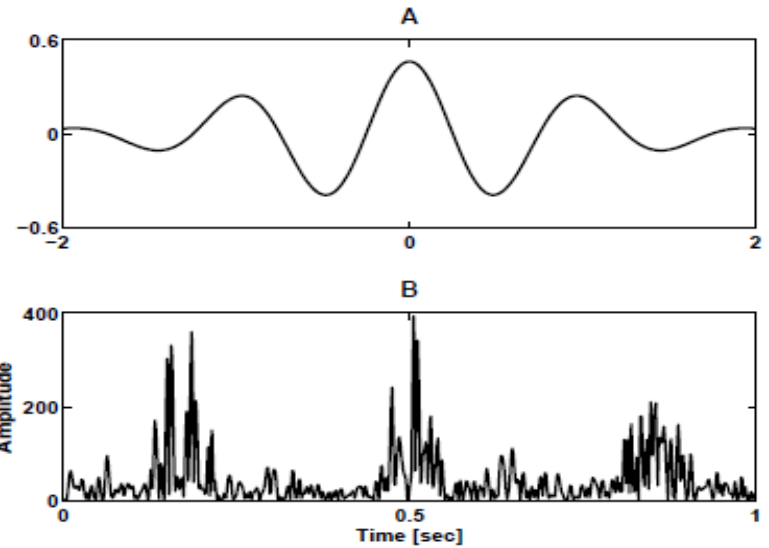
- The maximisation problem leads to the matrix eigenvalue equation

$$\sum_{t'}^N \frac{\sin[2\pi W(t-t')]}{\pi(t-t')} w_{t'} = \lambda w_t \quad (4.9)$$

- Eigen vector – Let A be a square matrix, a non-zero vector C is called a eigen vector of A if and only if there exists a number (real/complex) λ such that $AC = \lambda C$.

Lecture 4 – Different windows used for estimation

Extended Continuous Wavelet Transform Method



Extended Continuous Wavelet Transform Method

- If $x(t)$ is the signal then the continuous wavelet transform can be written as

$$CWT_x(\tau, a) = \frac{1}{a} \int x(t) h^* \left(\frac{t - \tau}{a} \right) dt \quad (4.10)$$

where h^* is the wavelet function and a is the scaling factor.

- The wavelet used in this method is the Morlet wavelet which is defined as

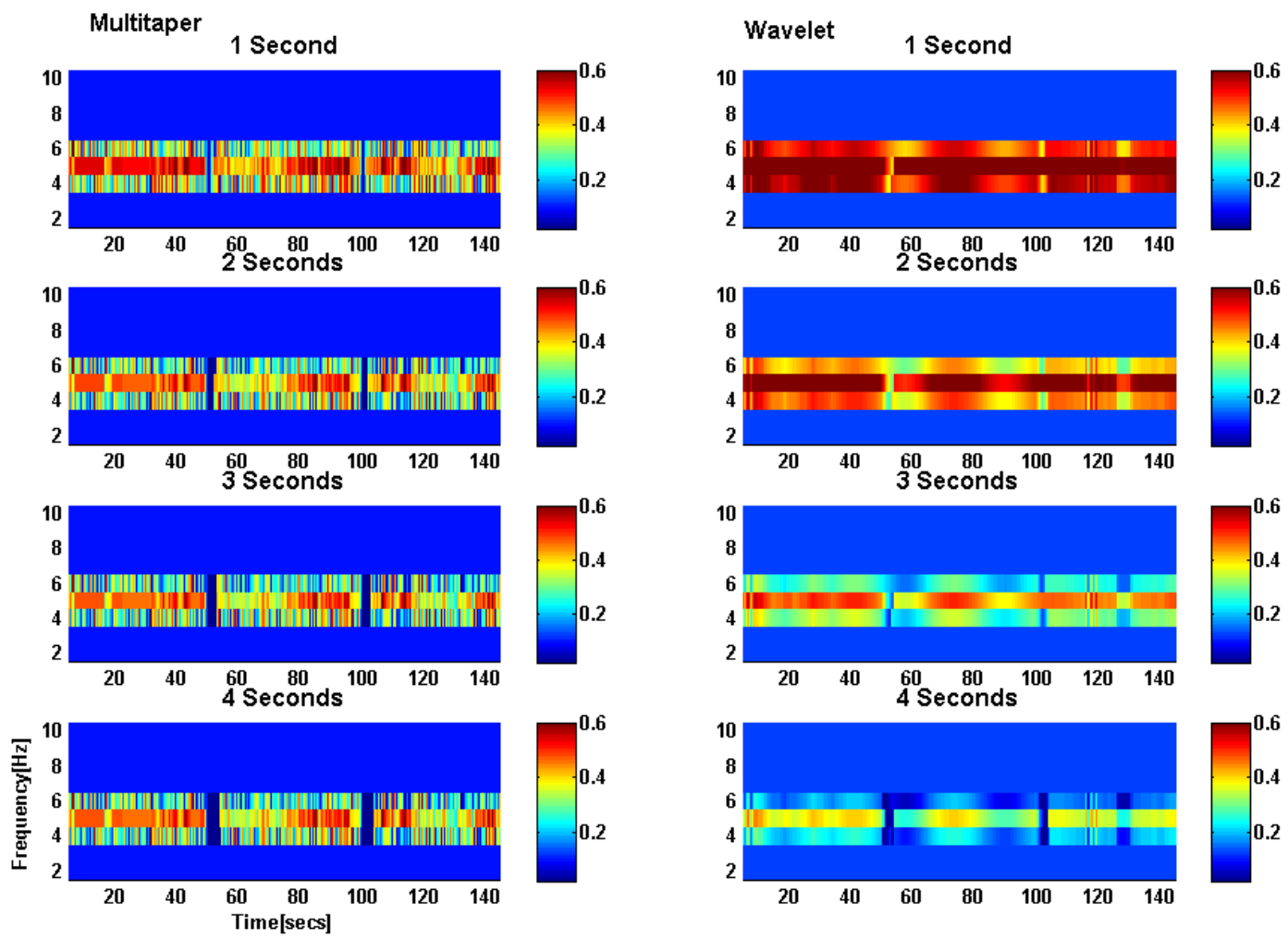
$$h(t) = \exp(jct) \exp(-\beta t^2/2) \quad (4.11)$$

- The relative bandwidth of this wavelet can be defined as

$$BW_{rel} = \frac{2\sqrt{2\beta}}{c} \quad (4.12)$$

- By adjusting the ratio of $\sqrt{\beta}/c$ which gives the flexibility in having a particular frequency resolution at a particular frequency.

Model data



Partial Coherence

- Let $x(t)$, $y(t)$ and $z(t)$ be three simultaneously measured signals of length N .
- The partial coherence is estimating by first calculating the power spectra S_{xx} , S_{yy} , S_{zz} and cross-spectra S_{xy} , S_{xz} and S_{yz} in each of the disjoint windows. Finally we average these quantities across all the segments to get the estimate of the same.
- We estimate the partial coherence between the signals $x(t)$, $y(t)$ and $z(t)$ as follows:

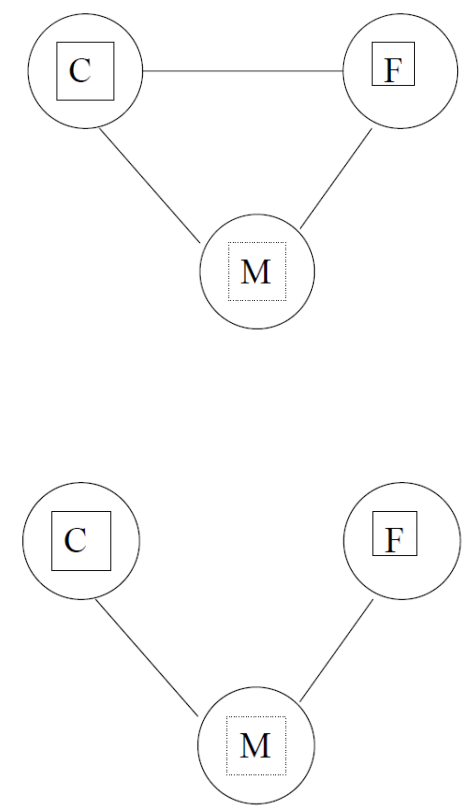
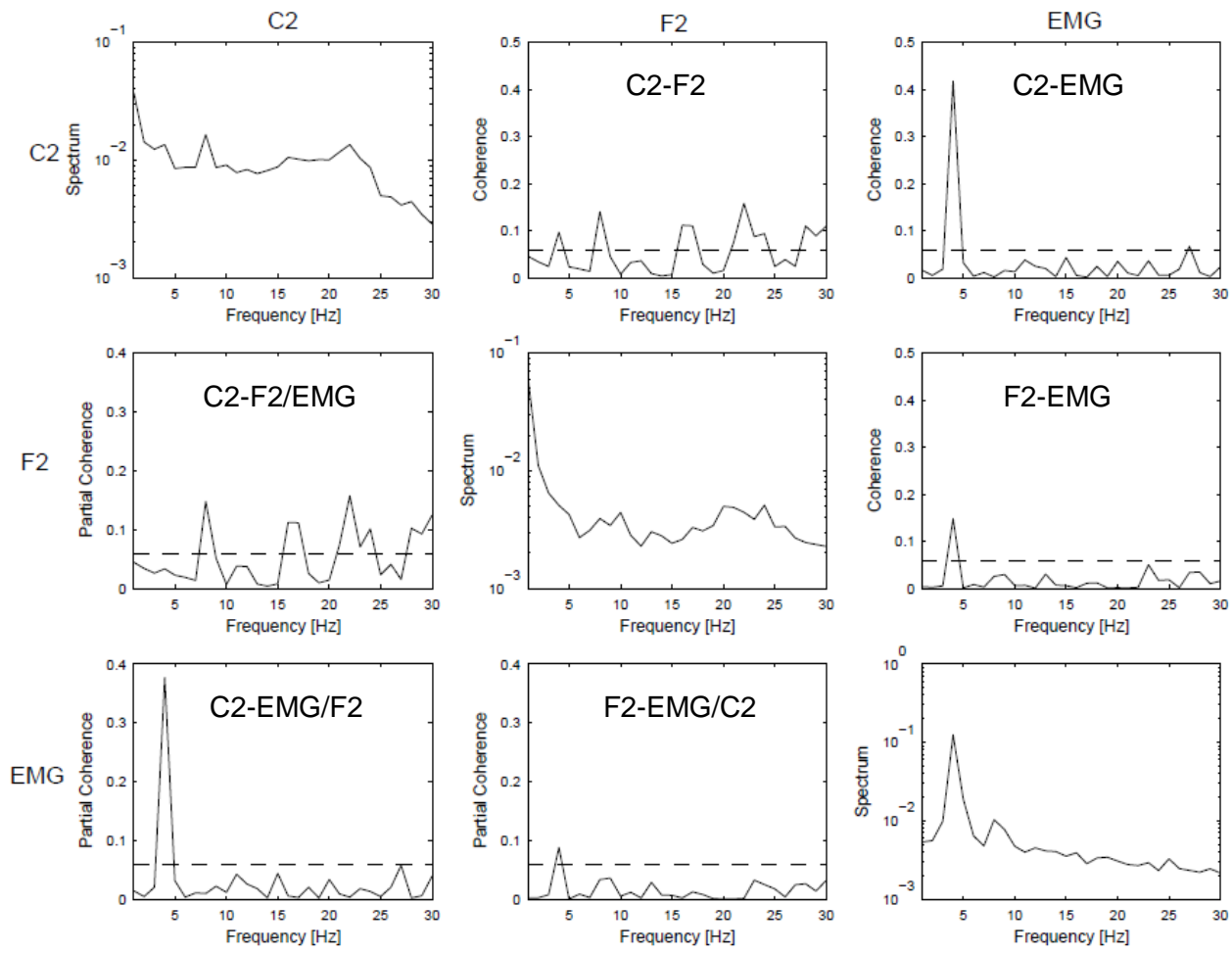
$$C_{xy/z}(\omega) = \frac{|CY_{xy}(\omega) - CY_{xz}(\omega)CY_{zy}(\omega)|^2}{(1 - C_{xz}(\omega))(1 - C_{zy}(\omega))} \quad (4.13)$$

where $CY_{ij}(\omega)$ is a complex-valued function whose magnitude is called coherency between the two signals i and j .

- The confidence limit for the partial coherence at 100% α is $1 - (1 - \alpha)^{1/(M-2)}$.

Lecture 4 – Different windows used for estimation

Partial Coherence



Lecture 4 – Different windows used for estimation

Methods for finding direction of information flow

Non-Parametric Methods	Parametric Methods (Based on modeling of system by linear VAR processes)
Partial Cross spectrum	Granger Causality Index
Partial Coherence	Directed Transfer Function
	Partial Directed Coherence

Partial Directed Coherence

- Partial directed coherence (PDC) can be formulated as follows:

$$x(t) = \sum_{r=1}^p a(r) \cdot x(t-r) + \eta(t) \quad (4.14)$$

$$A(\omega) = I - \sum_{r=1}^p a(r) \cdot e^{-i\omega r} \quad (4.15)$$

PDC:

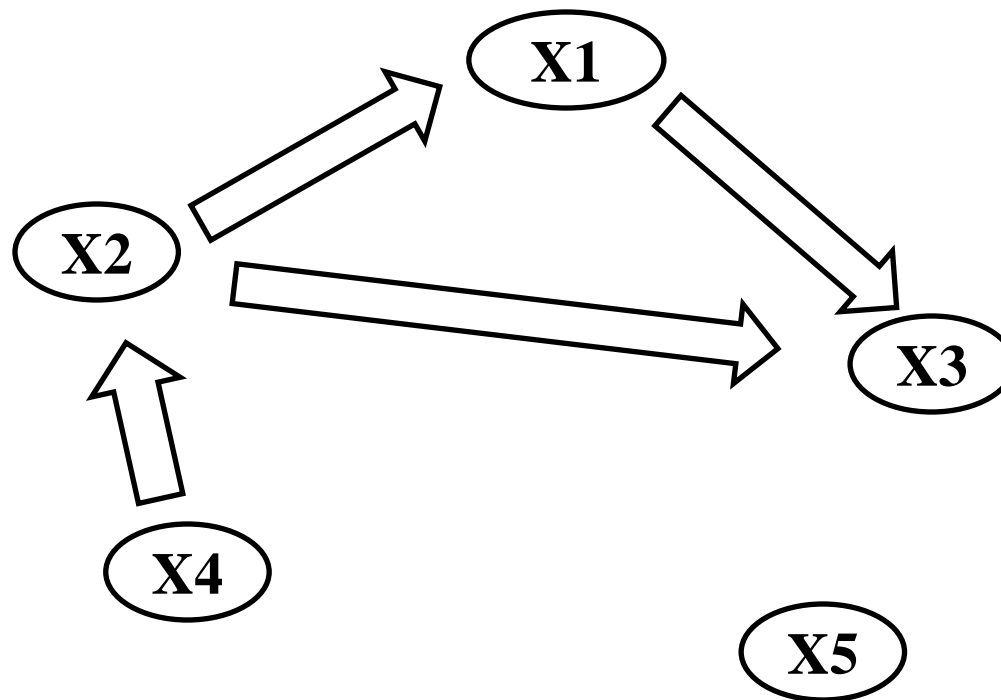
$$|\pi_{i \leftarrow j}(\omega)| = \frac{|A_{ij}(\omega)|}{\sqrt{\sum_k |A_{kj}(\omega)|^2}} \quad (4.16)$$

- In order to calculate PDC, we need to find the appropriate order ,p‘ for the underlying process.
- Optimum order can be found by Akaike Information Criterion (AIC).
- After finding the appropriate ,p‘, we need to find the coefficients for autoregressive model which closely depicts the process.

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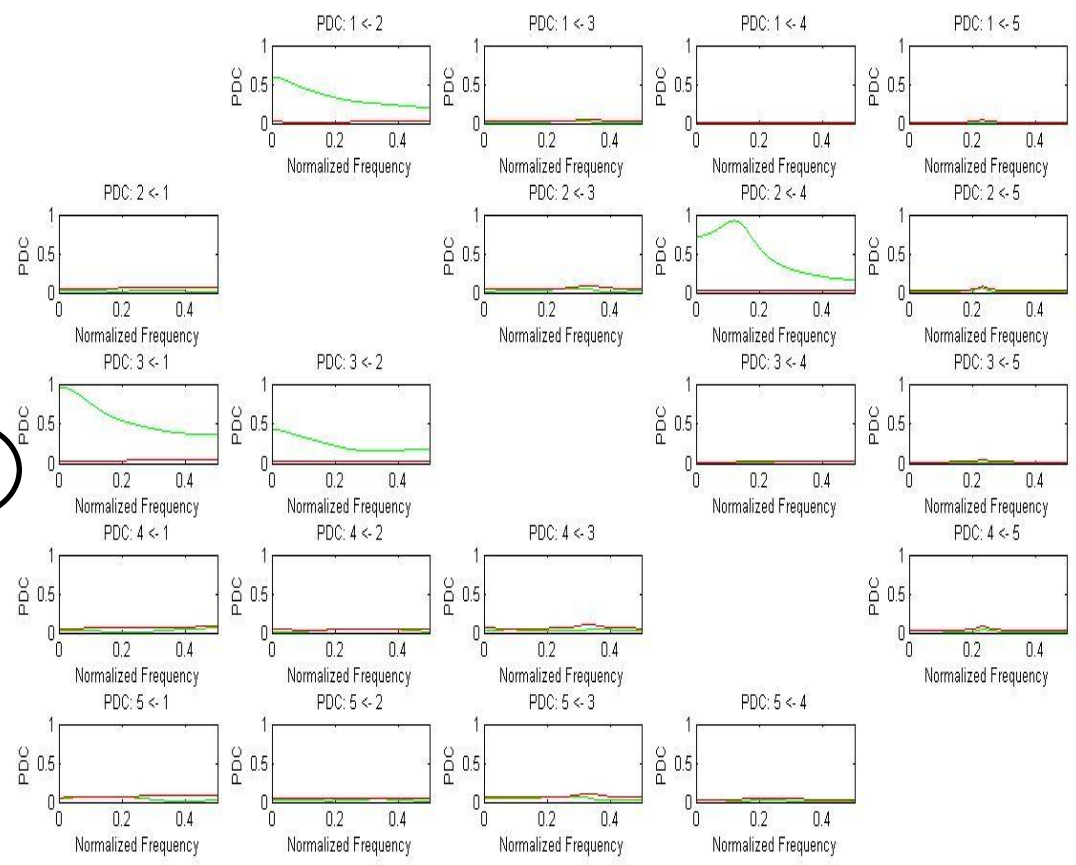
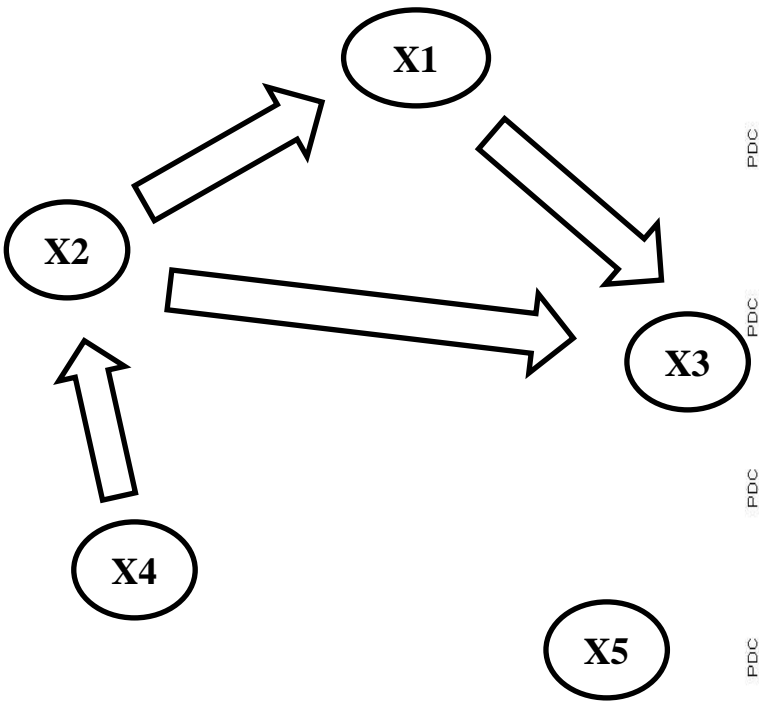
Partial Directed Coherence

- Application of PDC on model data with AR process of order $p=5$
- The five time series as the information flow between them as given in the figure below:



Lecture 4 – Different windows used for estimation

Partial Directed Coherence



Granger Causality Index

- The principle of Granger causality states that if some series $y(t)$ contains information in past terms that helps in the prediction of series $x(t)$, then $y(t)$ is said to cause $x(t)$.
- For predicting a value of $x(t)$ using p previous values of the series X only, we get a prediction error e :

$$X(t) = \sum_{i=1}^p A_{11}(j) X(t-j) + e(t) \quad (4.17)$$

- If we try to predict a value of $X(t)$ using p previous values of the series X and p previous values of Y we get another prediction error e_1 :

$$X(t) = \sum_{j=1}^p A_{11}(j) X(t-j) + \sum_{j=1}^p A_{12}(j) Y(t-j) + e_1(t) \quad (4.18)$$

- If the variance of e_1 (after including series Y to the prediction) is lower than the variance of e we say that Y causes X in the sense of Granger causality.

Granger Causality Index

- In the same way we can say that X causes Y in the sense of Granger causality when the variance of e_2 is reduced after including series X in the prediction of series Y :

$$Y(t) = \sum_{j=1}^p A_{22}(j) X(t-j) + \sum_{j=1}^p A_{21}(j) Y(t-j) + e_2(t) \quad (4.19)$$

- Granger causality index is based directly on the definition of causality, namely it shows, if the information contributed by second channel improves the prediction of the first channel.
- The logarithm ratio of the residual variances for one and two-channel models is computed:

$$GCI_{1 \rightarrow 2} = \ln(e/e_1) \quad (4.20)$$

- This definition can be extended to multichannel case by considering how the inclusion of the given channels changes the residual variance ratios.
- GCI is an estimator in the time domain.

Multivariate autoregressive Model

- Granger causality was defined for two channels, however, he later stated that the causality principle holds only, if there are no other channels influencing the process.
- To account for the whole multivariate structure of a process of k channels the multichannel autoregressive model (MVAR) has to be considered. For the MVAR k - channel process $X(t)$:

$$X(t) = (X_1(t), X_2(t), \dots, X_k(t)) \quad (4.21)$$

The model takes the form

$$X(t) = \sum_{i=1}^p A(i) X(t-i) + E(t) \quad (4.22)$$

where $E(t)$ are vectors of size k and the coefficients A are $k \times k$ - sized matrices

- Equation (4.22) can be easily transformed to describe relations in the frequency domain. After changing the sign of the A and application of Z transform we get:

$$E(f) = A(f) X(f) \quad (4.23)$$

Multivariate autoregressive Model

- It can be derived as follows:

$$X(f) = A^{-1}(f)E(f) = H(f)E(f) \quad (4.24)$$

$$H(f) = \left(\sum_{m=0}^p A(m) \exp(-2\pi i m f \Delta t) \right)^{-1} \quad (4.25)$$

- From the form of the above equations we can consider the model as a linear filter with white noises $E(f)$ on its input and the signals $X(f)$ on its output. The matrix of filter coefficients $H(f)$ is called the transfer matrix of the system.
- It contains information about all realtions between channels in the given set including the phase relations between the signals.

Directed Transfer Function

- The formulation of the DTF is based on the properties of the transfer function of multivariate autoregressive process as:

$$DTF_{j \rightarrow i}^2(f) = \frac{|H_{ij}(f)|^2}{\sum_{m=1}^k |H_{im}(f)|^2} \quad (4.24)$$

- The DTF describes causal influence of channel j on channel i at frequency f .
- The above equation defines a normalized version of DTF, which takes values from 0 to 1 producing a ration between the inflow of from channel j to channel i to all the inflows to channel i .